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=> d que stat 117
             1860 SEA FILE=HCAPLUS ABB=ON ?DEMINERAL? (W) ?BONE? (W) ?MATRIX? OR
L11
                83 SEA FILE=HCAPLUS ABB=ON L11 AND (?BONE?(W)?MORPHOGENET?(W)?PRO
L12
                    TEIN? OR ?COLLAGEN? (L) ?PROTEIN?)
                 7 SEA FILE=HCAPLUS ABB=ON L12 AND ?CROSSLINK?
L13
                 4 SEA FILE=HCAPLUS ABB=ON L13 AND ?COMPOSITION?
L16
                 7 SEA FILE=HCAPLUS ABB=ON L13 OR L16
L17
=> d ibib abs 117 1-7
L17 ANSWER 1 OF 7 HCAPLUS COPYRIGHT 2004 ACS on STN
ACCESSION NUMBER:
                               2003:1004968 HCAPLUS
DOCUMENT NUMBER:
                               140:8881
TITLE:
                               Allograft bone composition having a gelatin
                               binder
INVENTOR(S):
                               Merboth, Barbara L.; Sunwoo, Moon Hae; Gertzman,
                               Arthur A.
PATENT ASSIGNEE(S):
                               IJSA
                               U.S. Pat. Appl. Publ., 14 pp., Cont.-in-part of U.S.
SOURCE:
                               Ser. No. 983,526.
                               CODEN: USXXCO
                               Patent
DOCUMENT TYPE:
                               English
LANGUAGE:
FAMILY ACC. NUM. COUNT:
PATENT INFORMATION:
                                                     APPLICATION NO.
      PATENT NO.
                               KIND
                                        DATE
                               ----
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                                                       -----
      US 2002192263
                                A1
                                        20021219
                                                      US 2002-150097
                                                                                   20020520
                                                      US 1998-31750
      US 6030635
                               Α
                                        20000229
                                                                                    19980227
      US 6437018
                               B1
                                                      US 2000-515656
                                        20020820
                                                                                    20000229
                                                    US 2001-90322
WO 2003-US14534
BC BR, BY,
                               A1
      US 2003206937
                                        20031106
                                                                                    20011024
      WO 2003099236
          W: AE, AG, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, BZ, CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DZ, EC, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ, NO, NZ, OM, PH, PL, PT, RO, RU, SC, SD, SE, SG, SK, SL, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, YU, ZA, ZM, ZW, AM, AZ, BY, KG, KZ, MD, RU, TJ, TM
                               A1
                                        20031204
                                                                                   20030519
          RW: GH, GM, KE, LS, MW, MZ, SD, SL, SZ, TZ, UG, ZM, ZW, AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HU, IE, IT, LU, MC, NL, PT, RO, SE, SI, SK, TR, BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG
                                                       US 1998-31750
PRIORITY APPLN. INFO.:
                                                                               A2 19980227
                                                       US 1999-365880
                                                                               B2 19990803
                                                       US 2000-515656
                                                                               A2 20000229
                                                       US 2001-983526
                                                                                A2 20011024
                                                       US 2002-150097
                                                                               A 20020520
      The invention is directed toward an osteoimplant for application to a bone
AΒ
      defect site to promote new bone growth at the site which comprises a new
      bone growth inducing composition of demineralized allograft bone
      material mixed with an aqueous phosphate buffered gelatin which when
      lyophilized to remove water from the composition crosslinks
      the gelatin to form a solid structure. For example, a crosslinked
      gelatin bone formulation of 50% gelatin mixture, 40% demineralized
      bone matrix (DBM), and 10% of sodium
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hyaluronate paste was prepared 7.35. The formulation was wet with phosphate

buffered saline (PBS) pH = 7.35. The composition was flexible, strong, and slightly brittle. After freeze drying, the tissue was rehydrated with 10 mL PBS and at 60 min, it was slightly flexible with bone loosened around the ends.

L17 ANSWER 2 OF 7 HCAPLUS COPYRIGHT 2004 ACS on STN

ACCESSION NUMBER:

2003:202522 HCAPLUS

DOCUMENT NUMBER:

138:226801

TITLE: INVENTOR(S): A crosslinked collagen biomaterial Duneas, Nicolaas; Lutz, Martina Magdel

PATENT ASSIGNEE(S):

Bone SA, S. Afr.

SOURCE:

PCT Int. Appl., 19 pp.

CODEN: PIXXD2

DOCUMENT TYPE:

Patent English

LANGUAGE:

FAMILY ACC. NUM. COUNT:

PATENT INFORMATION:

	PATENT NO.			KIND DATE		APPLICATION NO.					DATE							
	WO	2003	0203	 27		A2	A2 20030313		WO 2002-IB3576					20020904				
	WO	2003	0203	27		A3		2004	0610									
		W:	ΑE,	AG,	AL,	AM,	AT,	AU,	AZ,	BA,	BB,	BG,	BR,	BY,	ΒZ,	CA,	CH,	CN,
			co,	CR,	CU,	CZ,	DE,	DK,	DM,	DZ,	EC,	EE,	ES,	FI,	GB,	GD,	GE,	GH,
			GM,	HR,	HU,	ID,	IL,	IN,	IS,	JP,	KE,	KG,	KP,	KR,	KZ,	LC,	LK,	LR,
				LT,														_
			PL,	PT,	RO,	RU,	SD,	SE,	SG,	SI,	SK,	SL,	TJ,	TM,	TN,	TR,	TT,	TZ,
			UA,	UG,	US,	UZ,	VC,	VN,	YU,	ZA,	ZM,	ZW,	AM,	AZ,	BY,	KG,	KZ,	MD,
			RU,	ТJ,	TM				•									
		RW:	GH,	GM,	KE,	LS,	MW,	MZ,	SD,	SL,	SZ,	TZ,	ŪĠ,	ZM,	ZW,	AT,	BE,	BG,
			CH,	CY,	CZ,	DE,	DK,	EE,	ES,	FI,	FR,	GB,	GR,	IE,	IT,	LU,	MC,	NL,
			PT,	SE,	SK,	TR,	BF,	ВJ,	CF,	CG,	CI,	CM,	GA,	GN,	GQ,	GW,	ML,	MR,
			NE,	SN,	TD,	TG	•	,		·	•	•	•	•				
	ZA	2002	0071	60 ·	•	Α		2003	0405		ZA 2	002-	7160			2	0020	905
PRIORITY APPLN. INFO.:								ZA 2	001-	7385		1	A 2	0010	906			

A method of producing a crosslinked collagen AB

biomaterial includes the step of providing a collagenous

biomaterial and irradiating the collagenous biomaterial with

 γ -irradiation at a dose of 20-160 kGy. The collagen

biomaterial is provided in the form of a gel and is produced by extracting bone powder or tendon. A composition comprising a crosslinked collagen gel 1000, together with bone

morphogenetic proteins 0.5-2.5 and demineralized

bone matrix 500 mg induced new bone formation when

injected into soft tissues of the rodent and bony sites of the human.

L17 ANSWER 3 OF 7 HCAPLUS COPYRIGHT 2004 ACS on STN

ACCESSION NUMBER:

2000:112616 HCAPLUS

DOCUMENT NUMBER:

132:330982

TITLE:

Proteolysis of human bone collagen by cathepsin K: characterization of the cleavage sites generating the

cross-linked N-telopeptide neoepitope

AUTHOR (S): CORPORATE SOURCE: Atley, L. M.; Mort, J. S.; Lalumiere, M.; Eyre, D. R. Orthopaedic Research Laboratories, University of

Washington, Seattle, WA, USA

SOURCE:

Bone (New York) (2000), 26(3), 241-247

CODEN: BONEDL; ISSN: 8756-3282

PUBLISHER:

Elsevier Science Inc.

DOCUMENT TYPE:

Journal

LANGUAGE:

English

An immunoassay for cross-linked N-telopeptides of type I collagen AB (NTx) in urine or serum has proven to give a sensitive index of osteoclast-mediated bone resorption. We show that recombinant human cathepsin K is highly active in releasing the NTx necepitope in 100% yield from bone type I collagen. Cathepsins S, L, and B were also active but at 57%, 36%, and 27% of the yield of K, resp. The matrix metalloproteinases that were tested, stromelysin, collagenase 3, or matrilysin, did not produce any immunoreactivity. Cathepsin K also acted on demineralized bone matrix, releasing NTx epitope and completely dissolving the bone particles in 24-48 h. Proteolytic cleavage of a G-L peptide bond in the $\alpha 2(I)N$ -telopeptide was shown to be required for recognition by monoclonal antibody 1H11. Peptide anal. identified bonds in the N-telopeptide and helical crosslinking domains adjacent to the crosslinking residues at which cathepsin K cleaved in bone collagen. The sites were consistent with the known substrate specificity of cathepsin K, which prefers a hydrophobic residue or proline in the critical P2 position. The NTx peptides generated by cathepsin K were of low mol. weight, in the range previously found in human urine. Because cathepsin K appears to be essential for the normal resorption of mineralized bone matrix by osteoclasts, these findings help explain the specificity and responsiveness of NTx as a marker of osteoclastic bone resorption in vivo.

REFERENCE COUNT:

47 THERE ARE 47 CITED REFERENCES AVAILABLE FOR THIS RECORD. ALL CITATIONS AVAILABLE IN THE RE FORMAT

L17 ANSWER 4 OF 7 HCAPLUS COPYRIGHT 2004 ACS on STN

ACCESSION NUMBER:

1998:624020 HCAPLUS

DOCUMENT NUMBER:

129:250241

TITLE:

Bone paste comprising a bioabsorbable osteogenic

compound in a gelatin matrix

INVENTOR (S):

Wironen, John F.; Grooms, Jamie M.

PATENT ASSIGNEE(S):

University of Florida Tissue Bank, Inc., USA; University of Florida Research Foundation, Inc.

PCT Int. Appl., 39 pp.

SOURCE:

CODEN: PIXXD2

DOCUMENT TYPE:

Patent

LANGUAGE:

English

FAMILY ACC. NUM. COUNT:

PATENT INFORMATION:

PA	PATENT NO. WO 9840113		KIND DATE			APPLICATION NO.					DATE						
WO				A1	_	1998	0917	1	WO 1	998-1	US49	04		1:	9980:	312	
	W:	AL,	AU,	BA,	BB,	BG,	BR,	CA,	CN,	CU,	CZ,	EE,	GE,	GW,	HU,	ID,	IL,
		IS,	JP,	KP,	KR,	LC,	LK,	LR,	LT,	LV,	MG,	MK,	MN,	MX,	NO,	NZ,	PL,
		RO,	SG,	SI,	SK,	SL,	TR,	TT,	UA,	US,	UZ,	VN,	YU,	AM,	AZ,	BY,	KG,
		KZ,	MD,	RU,	TJ,	TM											
	RW:	GH,	GM,	KE,	LS,	MW,	SD,	SZ,	ŪĠ,	ZW,	AT,	BE,	CH,	DE,	DK,	ES,	FI,
		FR,	GB,	GR,	ΙE,	IT,	LU,	MC,	NL,	PT,	SE,	BF,	ВJ,	CF,	CG,	CI,	CM,
		GA,	GN,	ML,	MR,	NE,	SN,	TD,	TG								
US	2002	0982	22		A1 20020725				US 1997-816079					19970313			
AU	9865	528			A1		1998	0929	1	AU 1	998-	6552	8		1:	9980	312
EP	9847	97			A1		2000	0315	1	EP 1	998-	9116	07		1:	9980	312
	R:	AT,	BE,	CH,	DE,	DK,	ES,	FR,	GB,	GR,	IT,	LI,	LU,	NL,	SE,	MC,	PT,
		ΙE,	FI														
JP	2001	5145	65		T2	:	2001	0911		JP 1	998-	5398:	19		1:	9980	312
PRIORITY APPLN. INFO.:			. :					Ţ	JS 1	997-	8160'	79	7	A 1	9970	313	
			•						7	WO 1	998-1	JS49	04	7	W 1	9980	312

AB A bone paste useful in the orthopedic arts, for example in the repair of

non-union fractures, periodontal ridge augmentation, craniofacial surgery, implant fixation, impaction grafting, or any other procedure in which generation of new bone is deemed necessary, is provided by a compn. comprising a substantially bioabsorbable osteogenic compound in a gelatin matrix. In various embodiments, the osteogenic compound is selected from (1) demineralized bone matrix (DBM

); (2) bioactive glass ceramic, Bioglass, bioactive ceramic, calcium phosphate ceramic, hydroxyapatite, hydroxyapatite carbonate, corraline hydroxyapatite, calcined bone, tricalcium phosphate, or like material; (3) bone morphogenetic protein, $TGF-\beta$, PDGF,

or mixts. thereof, natural or recombinant; and (4) mixts. of (1)-(3). The bone paste contains dry demineralized bone 0-40, lyophilized thermally crosslinkable gelatin 20-45, Bioglass 0-40%, and bone morphogenic protein 0.001 mg/mL. The bone paste was osteoinductive when implanted in rats.

REFERENCE COUNT: 11 THERE ARE 11 CITED REFERENCES AVAILABLE FOR THIS RECORD. ALL CITATIONS AVAILABLE IN THE RE FORMAT

L17 ANSWER 5 OF 7 HCAPLUS COPYRIGHT 2004 ACS on STN

ACCESSION NUMBER: 1996:455578 HCAPLUS

DOCUMENT NUMBER: 125:151095

TITLE: Comparative histological study of mineralizations

after intramuscular implantations of heat-denatured

demineralized bone matrix

gelatin, heat-denatured demineralized tooth, and

cross-linked collagen

AUTHOR(S): Ninomiya, Masami

CORPORATE SOURCE: Sch. Dent., Univ. Tokushima, Tokushima, 770, Japan

SOURCE: Shikoku Shigakkai Zasshi (1996), 9(1), 77-97

CODEN: SSZAED; ISSN: 0914-6091

PUBLISHER: Shikoku Shigakkai

DOCUMENT TYPE: Journal LANGUAGE: Japanese

AB

I.m. implantation of demineralized bone matrix gelatin (BMG) is known to form spherical mineralized deposits in the implant prior to bone tissue formation induced by bone morphogenetic protein (BMP). This type of mineralization is called "acellular mineral deposition (AMD)", which is not associated with osteogenic cells. In the present study, heat-denatured BMG, heat-denatured demineralized tooth, and calf skin type I collagen cross-linked with glutaraldehyde were resp. implanted into the rectus abdominis muscles in rats. Then mineralized deposits formed in the implants after the resp. implantations were compared by means of histol. anal.by using light and electron microscopes. Compns. of these deposits were also analyzed by electron probe x-ray microanal. Heat-denatured BMG, which was prepared at 150° for 30 min to inactivate non-collagenous proteins including BMP (NCP), was used to investigate whether NCP had some roles in AMD process. Heat-denatured demineralized tooth and crosslinked collagen were also used to examine the relations of AMD with calcification of dentin and with matrix collagen. In heat-denatured BMG, spherical mineralized deposits initially appeared at day 3 and then gradually increased in the size and the number Finally these deposits fused with each other to occupy the whole implant at day 14. Similar observations were obtained in the case of heat-denatured demineralized tooth implant. Mineralization was progressed in one way from enamel side to dental pulp side. Predentin area did not easily mineralized during the exptl. period. In crosslinked collagen, fiber-like mineralized deposits were scattered along collagen fiber bundles at day 3. These deposits gradually

increased in the number and invaded into the surrounding collagen fibers to increase in the size, and then these deposits fused with each other to occupy the whole implant at day 14. Bone and cartilaginous tissues did not appear around the implants, and also there were no osteoblast- and osteoclast-like cells in any implants. Mineralized deposits were formed compactly showing needle-shaped crystals in all implants. Composition anal. revealed that these deposits showed a similar mol. ratio of calcium to phosphorus. AMD occurs with no relation to the subsequent bone tissue formation and that NCP never have any roles in AMD process. AMD physicochem. occurs depending on cross-linked collagen of matrix and that AMD observed in the implanted dentin may take place in the physiol. mineralization because of the morphol. similarity between AMD and globular dentin.

L17 ANSWER 6 OF 7 HCAPLUS COPYRIGHT 2004 ACS on STN

ACCESSION NUMBER: 1994:621918 HCAPLUS

DOCUMENT NUMBER: 121:221918

TITLE: Effects of lathyritic drugs and lathyritic

demineralized bone matrix

on induced and sustained osteogenesis

AUTHOR(S): Di Cesare, Paul E.; Nimni, Marcel E.; Yazdi,

Mohamadreza; Cheung, David T.

CORPORATE SOURCE: Cartilage Bone Res. Cent., Hosp. Joint Dis.

Orthopaedic Inst., New York, NY, USA

SOURCE: Journal of Orthopaedic Research (1994), 12(3), 395-402

CODEN: JOREDR; ISSN: 0736-0266

DOCUMENT TYPE: Journal

LANGUAGE: English

AB Demineralized bone matrix was implanted in

normal and lathyritic rats. At 2 wk, the bone that formed in the lathyritic animals had an elevated alkaline phosphatase activity and a reduced calcium content compared with the controls. Four weeks after implantation, these biochem. parameters were reversed, with a decrease in alkaline phosphatase activity and an increase in calcium content to control levels. The histol. of the recovered implants revealed new bone formation. Lathyritic demineralized bone matrix was prepared from bones of rats fed β -aminopropionitrile

for 2 wk (2-wk BAPN-DBM) or 4 wk (4-wk BAPN-DBM), and was implanted in normal rats. Two weeks after implantation, both prepns. of lathyritic demineralized bone matrix

demonstrated early bone formation, although alkaline phosphatase activity and calcium content were reduced. By 4 wk after implantation, no biochem. or histol. evidence of bone formation remained at the site of the 4-wk BAPN-DBM implants; continued but reduced bone formation was observed at

the site of the 2-wk BAPN-DBM implants. Reconstitution of

inactivated normal demineralized bone matrix

with the guanidine-soluble exts. restored the osteoinductive capacity.

However, reconstitution of inactivated lathyritic demineralized

bone matrix (4-wk BAPN-DBM) failed to restore

the osteoinductive capacity. These results indicate that the degree of

crosslinking of the collagen matrix that acts as a

carrier for osteoinductive proteins plays a key role in inducing

and sustaining osteogenesis.

L17 ANSWER 7 OF 7 HCAPLUS COPYRIGHT 2004 ACS on STN

ACCESSION NUMBER: 1988:436094 HCAPLUS

DOCUMENT NUMBER: 109:36094

TITLE: Biochemical differences between dystrophic

calcification of cross-linked collagen implants and

mineralization during bone induction

AUTHOR(S): Nimni, Marcel E.; Bernick, Sol; Cheung, David T.;

Ertl, Delia C.; Nishimoto, Satoru K.; Paule, Wendelin

J.; Salka, Carl; Strates, Basil S.

CORPORATE SOURCE: Sch. Med., Univ. Southern California, Los Angeles, CA,

90007, USA

SOURCE: Calcified Tissue International (1988), 42(5), 313-20

CODEN: CTINDZ; ISSN: 0171-967X

DOCUMENT TYPE: Journal LANGUAGE: English

AB Ectopic calcification of diseased tissues or around prosthetic implants can lead to serious disability. Therefore, calcification of implants of glutaraldehyde-crosslinked collagenous tissues and reconstituted collagen was compared with mineralization induced by demineralized bone matrix (DBM

). Whereas implants of DBM accumulated large amts. of Ca and a bone-specific γ -carboxyglutamic acid **protein** (BGP or osteocalcin) following implantation in both young and older rats, implants of crosslinked pericardial tissue calcified with only traces of BGP. Glutaraldehyde-crosslinked DBM failed to calcify after implantation in 8-mo-old rats for 2-16 wk. Implants of crosslinked type I collagen exhibited small calcified deposits 2 wk postimplantation but Ca content eventually dropped to levels equal to those of soft tissues as the implants were resorbed. The Ca content of DBM implanted in 1- and 8-mo-old rats reached comparable levels after 4 wk, but the BGP content was approx. twice as high in the younger animals than in the older ones. Glutaraldehydecrosslinked implants of DBM, tendon, and cartilage calcified in young but not in old animals. This form of dystrophic calcification was associated with only trace amts. of BGP. Alkaline phosphatase

activity was high in implants of DBM and undetectable in implants of crosslinked collagenous tissues. These results show that implants of glutaraldehyde-crosslinked collagenous tissues and reconstituted collagen calcify to different extents depending upon their origin and the age of the host, and that the mechanism of dystrophic calcification differs from the process of mineralization associated with bone induction as reflected by alkaline

phosphatase activity and BGP accumulation.

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=> d que stat l19
           1860 SEA FILE=HCAPLUS ABB=ON ?DEMINERAL?(W)?BONE?(W)?MATRIX? OR
L11
             83 SEA FILE=HCAPLUS ABB=ON L11 AND (?BONE?(W)?MORPHOGENET?(W)?PRO
L12
                TEIN? OR ?COLLAGEN? (L) ?PROTEIN?)
L13
              7 SEA FILE=HCAPLUS ABB=ON L12 AND ?CROSSLINK?
L14
             10 SEA L13
              8 DUP REMOV L14 (2 DUPLICATES REMOVED)
L15
L18
              1 SEA L15 AND ?COMPOSIT?
L19
              8 SEA L15 OR L18
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L19 ANSWER 1 OF 8
                       MEDLINE on STN
ACCESSION NUMBER:
                    94267648
                                 MEDLINE
DOCUMENT NUMBER:
                    PubMed ID: 8207593
                    Effects of lathyritic drugs and lathyritic
TITLE:
                    demineralized bone matrix on
                    induced and sustained osteogenesis.
AUTHOR:
                    Di Cesare P E; Nimni M E; Yazdi M; Cheung D T
CORPORATE SOURCE:
                    Cartilage and Bone Research Center, Hospital for Joint
                    Diseases Orthopaedic Institute, New York, New York 10003.
CONTRACT NUMBER:
                    AG02577 (NIA)
     AM37042-01 (NIADDK)
                   Journal of orthopaedic research : official publication of
SOURCE:
                    the Orthopaedic Research Society, (1994 May) 12 (3)
                   395-402.
                    Journal code: 8404726. ISSN: 0736-0266.
PUB. COUNTRY:
                    United States
DOCUMENT TYPE:
                    Journal; Article; (JOURNAL ARTICLE)
LANGUAGE:
                    English
                    Priority Journals; Space Life Sciences
FILE SEGMENT:
                    199407
ENTRY MONTH:
ENTRY DATE:
                    Entered STN: 19940721
                    Last Updated on STN: 19940721
                    Entered Medline: 19940711
AB
     Demineralized bone matrix was implanted in
     normal and lathyritic rats. At 2 weeks, the bone that formed in the
     lathyritic animals had an elevated alkaline phosphatase activity and a
     reduced calcium content compared with the controls. Four weeks after
     implantation, these biochemical parameters were reversed, with a decrease
     in alkaline phosphatase activity and an increase in calcium content to
     control levels. The histology of the recovered implants revealed new bone
     formation. Lathyritic demineralized bone
     matrix was prepared from bones of rats fed beta-aminopropionitrile
     for 2 weeks (2-week BAPN-DBM) or 4 weeks (4-week BAPN-
     DBM), and was implanted in normal rats. Two weeks after
     implantation, both preparations of lathyritic demineralized
     bone matrix demonstrated early bone formation, although
     alkaline phosphatase activity and calcium content were reduced.
     weeks after implantation, no biochemical or histological evidence of bone
     formation remained at the site of the 4-week BAPN-DBM implants;
     continued but reduced bone formation was observed at the site of the
     2-week BAPN-DBM implants. Reconstitution of inactivated normal
     demineralized bone matrix with the
     guanidine-soluble extracts restored the osteoinductive capacity. However,
     reconstitution of inactivated lathyritic demineralized
    bone matrix (4-week BAPN-DBM) failed to
     restore the osteoinductive capacity. These results indicate that the
     degree of crosslinking of the collagen matrix that
```

acts as a carrier for osteoinductive proteins plays a key role in inducing and sustaining osteogenesis.

L19 ANSWER 2 OF 8 MEDLINE ON STN ACCESSION NUMBER: 90125632 MEDLINE DOCUMENT NUMBER: PubMed ID: 2612151

TITLE: Dystrophic calcification and mineralization during bone

induction: biochemical differences.

AUTHOR: Nimni M E; Bernick S; Ertl D C; Nishimoto S K; Paule W J;

Villanueva J

CORPORATE SOURCE: Department of Biochemistry, University of Southern

California School of Medicine, Los Angeles.

SOURCE: Connective tissue research, (1989) 20 (1-4) 193-204.

Journal code: 0365263. ISSN: 0300-8207.

Report No.: NASA-90125632.

PUB. COUNTRY: ENGLAND: United Kingdom

DOCUMENT TYPE: Journal; Article; (JOURNAL ARTICLE)

LANGUAGE: English

FILE SEGMENT: Priority Journals; Space Life Sciences

ENTRY MONTH: 199003

ENTRY DATE: Entered STN: 19900328

Last Updated on STN: 19900328 Entered Medline: 19900307

AB The calcification of implants of glutaraldehyde-cross linked

collagenous tissues and collagen was studied in young

and old rats and compared to bone induction by non-crosslinked

osteogenically active demineralized bone matrix (DBM). Glutaraldehyde-crosslinked

implants of DBM, tendon, and cartilage calcified in young but not in old animals and accumulated only trace amounts of BGP (Bone Gla protein, osteocalcin). Alkaline phosphatase activity and BGP was high in implants of DBM and undetectable in crosslinked implants. To try and understand why bone formation is so significantly

reduced in older Fischer 344 rats, we developed a system which consists of cylinders of DBM sealed at the ends with a Millipore filter.

Cells originating from 20 day old embryo donors were introduced into the chambers prior to subcutaneousmplantation. After 4 weeks of implantation in 26 month old rats, the cylinders containing embryonic calvaria or muscle cells were found to be full of bone and/or cartilage.

L19 ANSWER 3 OF 8 MEDLINE on STN ACCESSION NUMBER: 90010456 MEDLINE DOCUMENT NUMBER: PubMed ID: 2794638

TITLE: Dystrophic calcification and mineralization during bone

induction: biochemical differences.

AUTHOR: Nimni M E

CORPORATE SOURCE: Department of Biochemistry, University of Southern

California School of Medicine, Los Angeles.

SOURCE: Nippon Seikeigeka Gakkai zasshi, (1989 May) 63 (5) 630-42.

Journal code: 0413716. ISSN: 0021-5325.

Report No.: NASA-90010456.

PUB. COUNTRY: Japan

DOCUMENT TYPE: Journal; Article; (JOURNAL ARTICLE)

LANGUAGE: English

FILE SEGMENT: Priority Journals; Space Life Sciences

ENTRY MONTH: 198910

ENTRY DATE: Entered STN: 19900328

Last Updated on STN: 19900328 Entered Medline: 19891031

AB The calcification of implants of glutaraldehyde-crosslinked

collagenous tissues and collagen was studied in young and old rats and compared to bone induction by non-crosslinked osteogenically active demineralized bone matrix (DBM). Glutaraldehyde-crosslinked implants of DBM, tendon, and cartilage calcified in young but not in old animals and accumulated only trace amounts of BGP (Bone Gla protein, osteocalcin). Alkaline phosphatase activity was high in implants of DBM and undetectable in crosslinked implants. To try and understand why bone formation is so significantly reduced in older Fischer-344 rats, we developed a system which consists of cylinders of DBM sealed at the ends with a Millipore filter. Cells originating from 20-day-old embryo donors were introduced into the chambers prior to subcutaneous implantation. After 4 weeks of implantation in 26-month-old rats, the cylinders containing embryonic calvaria or muscle calls were found to be full of bone and/or cartilage.

L19 ANSWER 4 OF 8 BIOSIS COPYRIGHT (c) 2004 The Thomson Corporation. on STN

ACCESSION NUMBER: 1988:313408 BIOSIS

DOCUMENT NUMBER: PREV198886030446; BA86:30446

BIOCHEMICAL DIFFERENCES BETWEEN DYSTROPHIC CALCIFICATION OF TITLE:

CROSS-LINKED COLLAGEN IMPLANTS AND MINERALIZATION DURING

BONE INDUCTION.

AUTHOR (S): NIMNI M E [Reprint author]; BERNICK S; CHEUNG D T; ERTL D

C; NISHIMOTO S K; PAULE W J; SALKA C; STRATES B S

2400 S FLOWER ST, LOS ANGELES, CALIF 90007-2697, USA CORPORATE SOURCE:

SOURCE:

Calcified Tissue International, (1988) Vol. 42, No. 5, pp.

313 - 320.

CODEN: CTINDZ. ISSN: 0171-967X.

DOCUMENT TYPE: Article FILE SEGMENT: RΔ LANGUAGE: ENGLISH

ENTRY DATE: Entered STN: 3 Jul 1988

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Ectopic calcification of diseased tissues or around prosthetic implants can lead to serious disability. Therefore, calcification of implants of glutaraldehyde-cross-linked collagenous tissues and reconstituted collagen was compared with mineralization induced

by demineralized bone matrix (DBM). Whereas implants of DBM accumulated larger amounts of calcium and a bone-specific-γ-carboxyglutamic acid protein (BGP or osteocalcin) following implantation in both young and older rats, implants of cross-linked pericardium calcified with only traces of BGP. Glutaraldehdye-cross-linked DBM failed to calcify after implantation in 8-month-old rats for 2-16 weeks. crosslinked type I collagen exhibited small calcific deposits 2 weeks postimplantation but calcium content eventually dropped to levels equal to those of soft tissues as the implants were resorbed. The calcium content of DBM implanted in 1- and 8-month-old rats reached comparable levels after 4 weeks, but the BGP content was approximately twice as high in the younger animals than in the older ones. Glutaraldehyde-cross-linked implants of DBM, tendon, and cartilage calcified significantly in young but not in old animals. This form of dystrophic calcification was associated with only trace amounts of BGP. Alkaline phosphatase activity was high in implants of DBM and undetectable in implants of cross-linked collagenous tissues. These results show that implants of glutaraldehyde-cross-linked collagenous tissues and reconstituted collagen calcify to different extents depending upon their origin and the age of the host, and that the mechanism of dystrophic calcification differs significantly from the process of mineralization associated with bone inductions as

reflected by alkaline phosphatase activity and BGP accumulation.

L19 ANSWER 5 OF 8 EMBASE COPYRIGHT 2004 ELSEVIER INC. ALL RIGHTS RESERVED.

on STN

ACCESSION NUMBER: 1999261735 EMBASE

TITLE: Osteogenesis imperfecta: Bone turnover, bone density, and

ultrasound parameters.

AUTHOR: Cepollaro C.; Gonnelli S.; Pondrelli C.; Montagnani A.;

Martini S.; Bruni D.; Gennari C.

CORPORATE SOURCE: C. Cepollaro, Institute of Internal Medicine, University of

Siena, Viale Bracci 2, Siena, Italy

SOURCE: Calcified Tissue International, (1999) 65/2 (129-132).

Refs: 24

ISSN: 0171-967X CODEN: CTINDZ

COUNTRY: DOCUMENT TYPE: United States
Journal; Article

FILE SEGMENT:

006 Internal Medicine

LANGUAGE: English SUMMARY LANGUAGE: English

We studied 21 patients (11 men and 10 women) with osteogenesis imperfecta (OI) and 21 age- and sex-matched controls. In all patients we measured serum levels of total alkaline phosphatase (ALP), type I procollagen carboxy-terminal propeptide (PICP), osteocalcin (BGP), urinary excretion of hydroxyproline (HOP/Cr), and pyridinoline crosslinks (Pyr/Cr). Bone mineral density was measured at the distal radius (BMD-R) and at the lumbar spine (BMD-LS) by dual X-ray absorptiometry (DXA). Ultrasound parameters were also performed at the calcaneous with the Achilles device and at the phalanxes with DBM Sonic 1200. A significant reduction (P < 0.001) in BMD and in ultrasound parameters was found in OI patients compared with normals. PICP was significantly reduced in the OI patients compared with controls (P < 0.001); other markers of bone turnover were higher in OI than in controls, but the difference did not reach the statistical significance. A significant correlation (P < 0.05) was found between PICP and BMD at the lumbar spine and between PICP and ultrasound parameters at the calcaneous. On the basis of our data, we conclude that patients with OI show low values of BMD and ultrasound parameters; therefore in these patients, not only is bone mass disturbed but also bone quality. The reduced levels of PICP in OI patients confirm that most OI patients have defects in collagen I biosynthesis. These defects may contribute to the fragility of OI bone by interfering with complete mineralization and/or normal tissue structure. PICP may be considered a useful marker in the clinical management of OI.

L19 ANSWER 6 OF 8 WPIDS COPYRIGHT 2004 THE THOMSON CORP on STN

ACCESSION NUMBER: 2002-682664 [73] WPIDS

DOC. NO. NON-CPI:
DOC. NO. CPI:

N2002-539008 C2002-192528

TITLE:

Injectable bone like implant used for repairing bone defect and injury comprises bone like compound and

hydrophobic carrier or degradable component.

DERWENT CLASS:

A96 B04 D22 P34

INVENTOR(S):

WIRONEN, J F

PATENT ASSIGNEE(S):

(WIRO-I) WIRONEN J F; (REGE-N) REGENERATION TECHNOLOGIES

INC

COUNTRY COUNT:

97

PATENT INFORMATION:

RW: AT BE CH CY DE DK EA ES FI FR GB GH GM GR IE IT KE LS LU MC MW MZ

NL OA PT SD SE SL SZ TR TZ UG ZM ZW

W: AE AG AL AM AT AU AZ BA BB BG BR BY BZ CA CH CN CO CR CU CZ DE DK

DM DZ EE ES FI GB GD GE GH GM HR HU ID IL IN IS JP KE KG KP KR KZ LC LK LR LS LT LU LV MA MD MG MK MN MW MX MZ NO NZ PL PT RO RU SD

SE SG SI SK SL TJ TM TR TT TZ UA UG UZ VN YU ZA ZW

US 2002193883 A1 20021219 (200303)

A2 20031112 (200377) EN EP 1359951

R: AL AT BE CH CY DE DK ES FI FR GB GR IE IT LI LT LU LV MC MK NL PT

RO SE SI TR

AU 2002251861 A1 20020806 (200427)

APPLICATION DETAILS:

PATENT NO	KIND	APPLICATION	DATE
WO 2002058755	A2	WO 2002-US3092	20020125
US 2002193883	A1 Provisional	US 2001-263972P	20010125
		US 2002-56217	20020125
EP 1359951	A2	EP 2002-720893	20020125
		WO 2002-US3092	20020125
AU 2002251861	A1	AU 2002-251861	20020125

FILING DETAILS:

PATENT NO	KIND	PATENT NO
EP 1359951	A2 Based on	WO 2002058755
AU 2002251861	A1 Based on	WO 2002058755

PRIORITY APPLN. INFO: US 2001-263972P 20010125; US 2002-56217 20020125

2002-682664 [73] WPIDS AΝ WO 200258755 A UPAB: 20021113 AB

> NOVELTY - A bone-like implant comprises at least one bone-like compound and a hydrophobic carrier or at least one degradable component.

> DETAILED DESCRIPTION - An INDEPENDENT CLAIM is included for production of the implant which comprises mixing at least one bone-like compound in a hydrophobic carrier or a degradable component and concurrently or subsequently combining with an aqueous phase to form a combined mixture.

ACTIVITY - Osteopathic.

MECHANISM OF ACTION - None given in the source material.

USE - Used for repairing a bone defect and injury.

ADVANTAGE - The implant is capable of aqueous sintering or curing and increasing its porosity in situ. Dwg.0/0

L19 ANSWER 7 OF 8 WPIDS COPYRIGHT 2004 THE THOMSON CORP on STN.

ACCESSION NUMBER: 1999-326321 [27] WPIDS

1989-178217 [24] CROSS REFERENCE: N1999-244804 DOC. NO. NON-CPI: DOC. NO. CPI: C1999-096403

TITLE: Production of biocompatible delivery systems for repair

of osseous defects.

DERWENT CLASS: A96 B04 B07 C03 C07 P32

INVENTOR(S): JEFFERIES, S R

PATENT ASSIGNEE(S): (BIOC-N) BIOCOLL LAB INC

COUNTRY COUNT:

PATENT INFORMATION:

PATENT NO	KII	Œ	DATE		WEEK	LA	I	PG
								-
US 5904718	Α	19	9990518	(1	199927) *		12	

APPLICATION DETAILS:

PATENT NO	KIND	APPLICATION	DATE
US 5904718	A Cont of CIP of Cont of Cont of Cont of Cont of Cont of Cont of Div ex CIP of	US 1986-844886 US 1987-80145 US 1987-119916 US 1991-718914 US 1992-892646 US 1993-57951 US 1995-422745 US 1995-470368 US 1997-872210	19860327 19870630 19871113 19910624 19920602 19930129 19950414 19950606 19970609

PRIORITY	APPLN.	INFO:	US 1997-872210	19970609;	US
			1986-844886	19860327; US	
			1987-80145	19870630; US	
			1987-119916	19871113; US	
			1991-718914	19910624; US	
			1992-892646	19920602; US	
			1993-57951	19930129; US	
			1995-422745	19950414; US	
			1995-470368	19950606	

AN 1999-326321 [27] WPIDS

CR 1989-178217 [24]

AB US 5904718 A UPAB: 19990714

NOVELTY - Method uses collagen and demineralized bone particles. It may contain a maximum of 20 % inorganic materials. The product is densified by compression, and additional osteogenic factors, mitogens, drugs or antibiotics may be incorporated in it. Inorganic materials may be bound to the organic matrix via pre-coating with a calcium or hydroxyapatite binding protein, peptide or amino acid. The materials display long lasting drug release characteristics.

DETAILED DESCRIPTION - Methods of making biocompatible delivery system comprise (a) dispersing bioactive protein, peptide or drug with protein particles chosen from demineralized bone matrix optionally extracted in chaotropic agents and/or reconstituted collage; (b) dispersing the particles in an aqueous solution of 0.002-0.25 weight % crosslinking agent and surface activating or partially crosslinking the particles; (c) removing the particles from the aqueous dispersion; and (d) adding organic matrix to the particles. An INDEPENDENT CLAIM is also included for a similar method of making biocompatible delivery system in which the bioactive protein, peptide or drug is dispersed within coated inorganic particles with a protein-based surface layer bound to them.

USE - Used to manufacture biocompatible delivery systems (claimed). Used to manufacture protein-based structures that delivery drugs or other agents including antibiotics, bone morphogenetic protein, insulin-like growth factor, nerve growth factor and human, bovine or porcine growth hormones in a controlled and stable manner. Used to prepare bone repair materials.

ADVANTAGE - Method improves binding and reactivity of **protein** -based or -coated particles to organic matrixes. Materials display lasting drug-release characteristics. Bone repair materials have improved

cohesive and physical strength for use in stress-bearing defects or where the ability to produce and maintain the specific shape of an implant is important. Inorganic particles in the materials are not easily displaced or dislodged from the matrix. Materials induce bone when implanted into animals or humans and have stress-bearing properties early after implantation.

Dwg.0/0

L19 ANSWER 8 OF 8 WPIDS COPYRIGHT 2004 THE THOMSON CORP on STN

ACCESSION NUMBER: 1998-506489 [43] WPIDS

DOC. NO. NON-CPI: N1998-394814 DOC. NO. CPI: C1998-152868

TITLE: Implantable bone paste for inducing new bone growth -

comprises gelatin matrix and bio-absorbable osteogenic

compound, especially demineralised bone

matrix.

DERWENT CLASS: B04 D22 L02 P34

INVENTOR(S): GROOMS, J M; WIRONEN, J F

PATENT ASSIGNEE(S): (UYFL) UNIV FLORIDA RES FOUND INC; (UYFL-N) UNIV FLORIDA

TISSUE BANK INC; (GROO-I) GROOMS J M; (WIRO-I) WIRONEN J

F

COUNTRY COUNT: 73

PATENT INFORMATION:

PAT	TENT NO	KIND DATE	WEEK	. LA	PG		
WO	9840113	A1 19980917	(199843)	* EN	39		
	RW: AT BE CH	DE DK EA ES	FI FR GB	GH GM	GR IE IT	KE LS LU	MC MW NL OA
	PT SD SE	SZ UG ZW					
	W: AL AU BA	BB BG BR CA	CN CU CZ	EE GE	GW HU ID	IL IS JP	KP KR LC LK
	LR LT LV	MG MK MN MX	NO NZ PL	RO SG	SI SK SL	TR TT UA	US UZ VN YU
AU	9865528	A 19980929	(199906)				
EP	984797	A1 20000315	(200018)	EN			
	R: AT BE CH	DE DK ES FI	FR GB GR	IE IT	LI LU MC	NL PT SE	
CZ	9903236	A3 20000816	(200048)				
SK	9901257	A3 20000814	(200051)				
HU	2000001811	A2 20001030	(200064)				
JP	2001514565	W 20010911	(200167)		38		
ΑU	2002022995	A 20020502	(200236)‡	ŧ			
US	2002098222	A1 20020725	(200254)				

APPLICATION DETAILS:

PATENT NO	KIND	APPLICATION	DATE
WO 9840113	A1	WO 1998-US4904	19980312
AU 9865528	A	AU 1998-65528	19980312
EP 984797	A1	EP 1998-911607	19980312
		WO 1998-US4904	19980312
CZ 9903236	A3	WO 1998-US4904	19980312
		CZ 1999-3236	19980312
SK 9901257	A3	WO 1998-US4904	19980312
		SK 1999-1257	19980312
HU 2000001811	A2	WO 1998-US4904	19980312
		HU 2000-1811	19980312
JP 2001514565	W	JP 1998-539819	19980312
		WO 1998-US4904	19980312
AU 2002022995	A Div ex	AU 1998-65528	19980312
		AU 2002-22995	20020307
US 2002098222	A1	US 1997-816079	19970313

FILING DETAILS:

PATENT NO	KIND	PATENT NO
AU 9865528	A Based on	WO 9840113
EP 984797	Al Based on	WO 9840113
CZ 9903236	A3 Based on	WO 9840113
HU 2000001811	A2 Based on	WO 9840113
JP 2001514565	W Based on	WO 9840113

PRIORITY APPLN. INFO: US 1997-816079 19970313; AU 2002-22995 20020307

AN 1998-506489 [43] WPIDS

AB WO 9840113 A UPAB: 19981028

An implantable bone paste composition comprises gelatin as a carrier for substantially bioabsorbable osteogenic components for use in a patient in need of new bone growth.

The gelatin is thermally **crosslinkable** at or slightly above the temperature of the organism into which it is to be implanted, preferably about 38 deg. C, and is in amount 20-45 weight%.

The osteogenic component is selected from:

(i) demineralised bone matrix (
DBM);

(ii) bioactive glass ceramic, BIOGLASS (RTM), bioactive ceramic, calcium phosphate ceramic, hydroxyapatite, hydroxyapatite carbonate, corraline hydroxyapatite, calcined bone, tricalcium phosphate or mixtures;

(iii) bone morphogenetic protein,

TGF-beta, PDGF or mixtures, natural or recombinant; and

(iv) mixtures of (i) - (iii).

The gelatin, the demineralised bone matrix or both are derived from the species into which the bone paste is to be implanted.

The DBM is in amount 0-40 (preferably 15-33) weight%.

The bioactive glass is BIOGLASS (RTM), especially of diameter 0.5-710 $\,$ mm.

Component (ii) is in amount 0-40 wt.%.

The composition comprises antibiotics, bone morphogenetic or other proteins, whether derived from natural or recombinant sources, wetting agents, glycerol, carboxymethyl cellulose (CMC), growth factors, steroids, non-steroidal anti-inflammatory compounds or combinations, and comprises 0.0001-0.1 mg/ml bone morphogenetic protein.

The composition is freeze dried.

The gelatin is human, bovine, ovine, equine, canine or mixtures, preferably derived from human **collagen** sources (especially human skin, bone, cartilage, tendon, connective tissue or mixtures) via enzymatic, acid or alkaline extraction. The gelatin has a molecular weight greater than 50,000 daltons.

Preferably, the osteogenic component is powdered DBM, in amount 0-40 wt.*, with particles of size 80-850 mm diameter, provided that if the DBM is absent, then a bone growth factor (especially morphogenetic protein, TGF-b or mixtures) is present at a concentration of at least 0.0001 mg/ml.

The composition further comprises cortical, cancellous or cortical and cancellous bone chips, of size 80 mm to 10 mm.

cortical and cancellous bone chips, of size 80 mm to 10 mm.

USE - For inducing bone formation in vivo, e.g. repair of non-union fractures, periodontal ridge augmentation, arthrodesis of spinal or other joints, spinal fusion procedures and implant fixation (all claimed); also in craniofacial surgery and impaction grafting.

ADVANTAGE - The bone paste is easy to handle and store, adheres to the implantation site, is both osteo-conductive and osteoinductive, is thermally **crosslinkable** and bioabsorbable. Dwg.0/4